

## Background

- ❖ 95% of amputees in developing countries do not have access to prosthetic care<sup>1</sup>
- ❖ Creating a high quality, well-fitted prosthetic socket is a labor-intensive process that takes several months and thousands of dollars to develop
- ❖ The shape of the residual limb also undergoes many changes throughout the amputee's lifetime, so the cost of getting an artificial limb is unsustainable

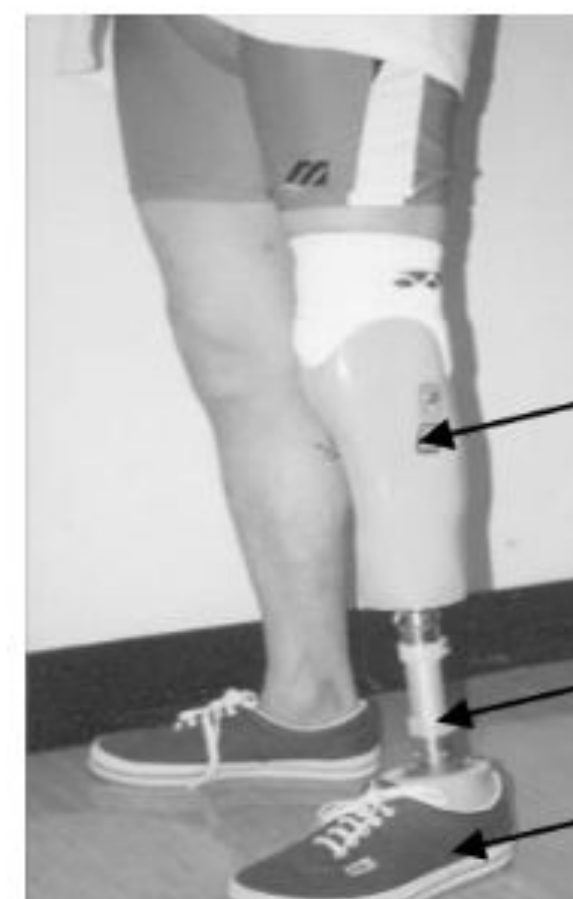


Figure 1. A typical transtibial prosthetic leg<sup>2</sup>.



Figure 2. Prosthetist casting a mold of the residual limb<sup>3</sup>.

## Objectives

- ❖ Our aim was to be able to use 3D residual limb models created from cell phone photogrammetry to create an affordable, well-fit prosthetic socket
  - Become familiar with Autodesk Meshmixer
  - Come up with design iterations from literature
  - 3D print and test socket designs
  - Come up with a final design and write a procedure

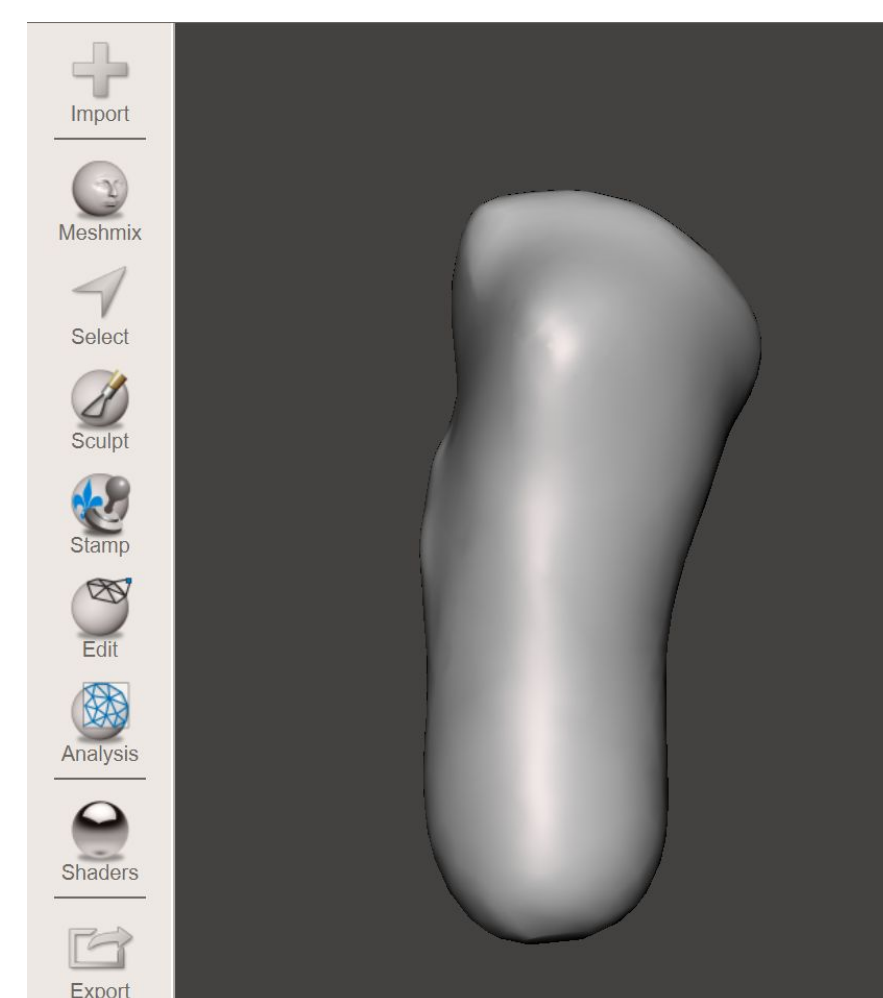


Figure 3. Residual Limb Model Using Autodesk MeshMixer.



Figure 4. Example of 3D printed socket<sup>3</sup>.

## Acknowledgements

We would like to thank Isaac Cabrera for his continuous guidance and Albert Lin for his unwavering support.  
We would also like to thank the McKittrick lab, MAE Department, Qualcomm Institute, Center for Human Frontiers, and Engineers Without Borders.

## Design Considerations

- ❖ Shape of the socket: Patellar tendon bearing (PTB) vs total surface bearing (TSB)
- ❖ Pressure distribution: Loading and unloading zones on the residual limb
- ❖ Suspension system: Passive vs active suction, low cost cuffs and belts
- ❖ Socket-pylon attachment: Where failure occurs most of the time

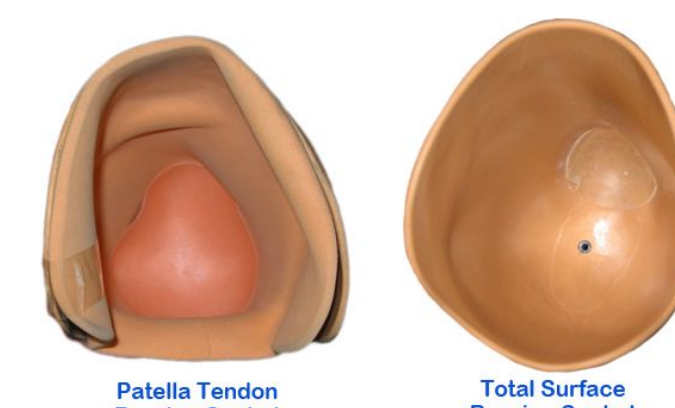


Figure 5. Interior of PTB socket (left) and TSB socket (right)<sup>4</sup>.

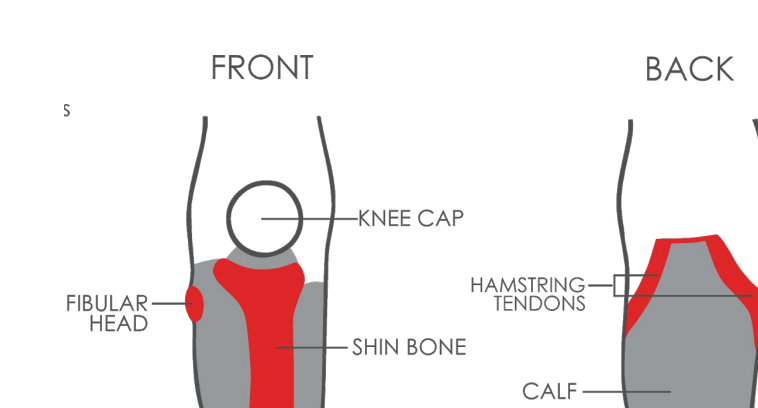


Figure 6. Pressure zones for a transtibial residual limb<sup>5</sup>.

## Design Iterations

- ❖ First and second designs were created by following the procedure written previously
- ❖ Cylinder for attachment of a one-way check valve for passive suction suspension
- ❖ Created a lip on socket anterior so the back of the knee doesn't hit the socket when bending
- ❖ Changed socket-ylon attachment from a rectangular shape to cylindrical for smoother print and more even stress distribution
- ❖ Incorporated a supracondylar socket shape for better suspension
- ❖ Joined socket bottom and pylon attachment for a smoother print

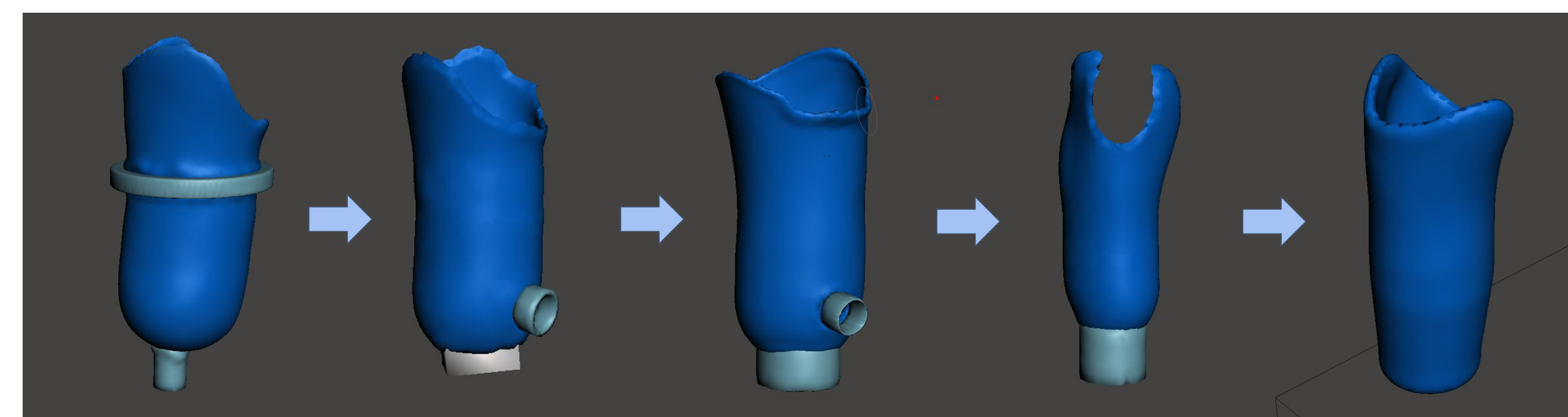


Figure 7. Progression of design iterations.

*Final design*

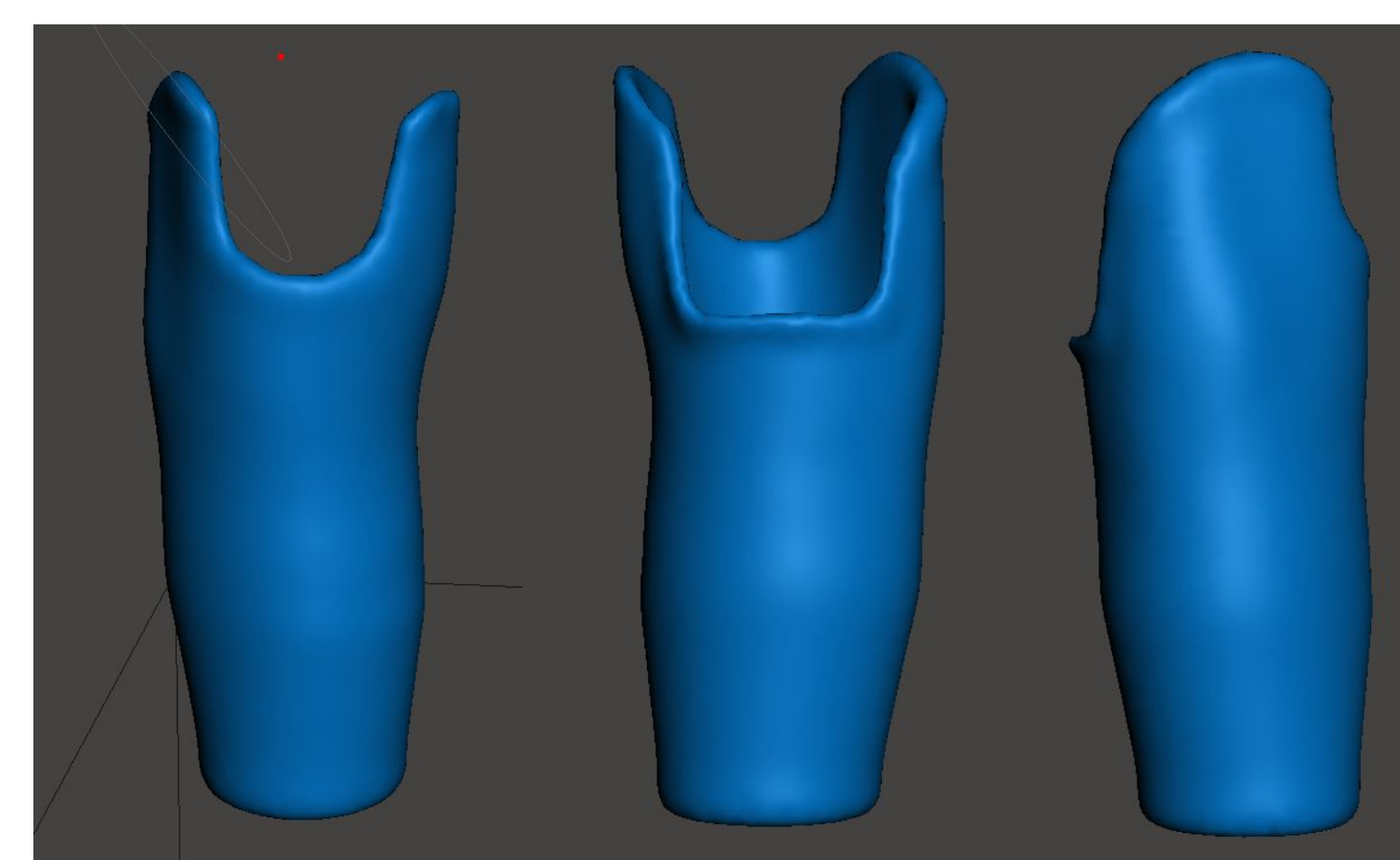


Figure 8. Frontal (left), dorsal (middle) and lateral (right) view of the final socket design.

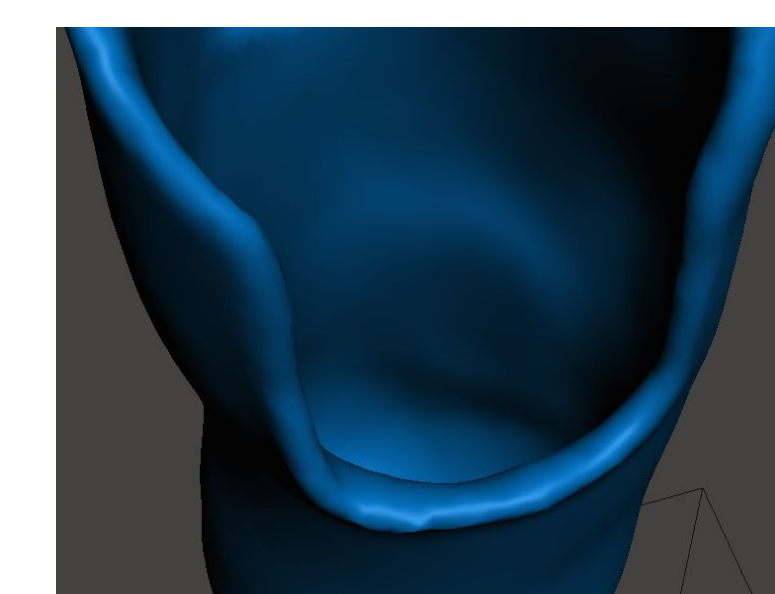


Figure 9. Interior of final socket showing pressure areas.

- ❖ Extended sides similar to supracondylar socket and prosthetist's socket
- ❖ Smoother and flatter lip for better print quality
- ❖ Included raised areas in the interior socket to help with pressure distribution

## Results

### 3D Printed Sockets

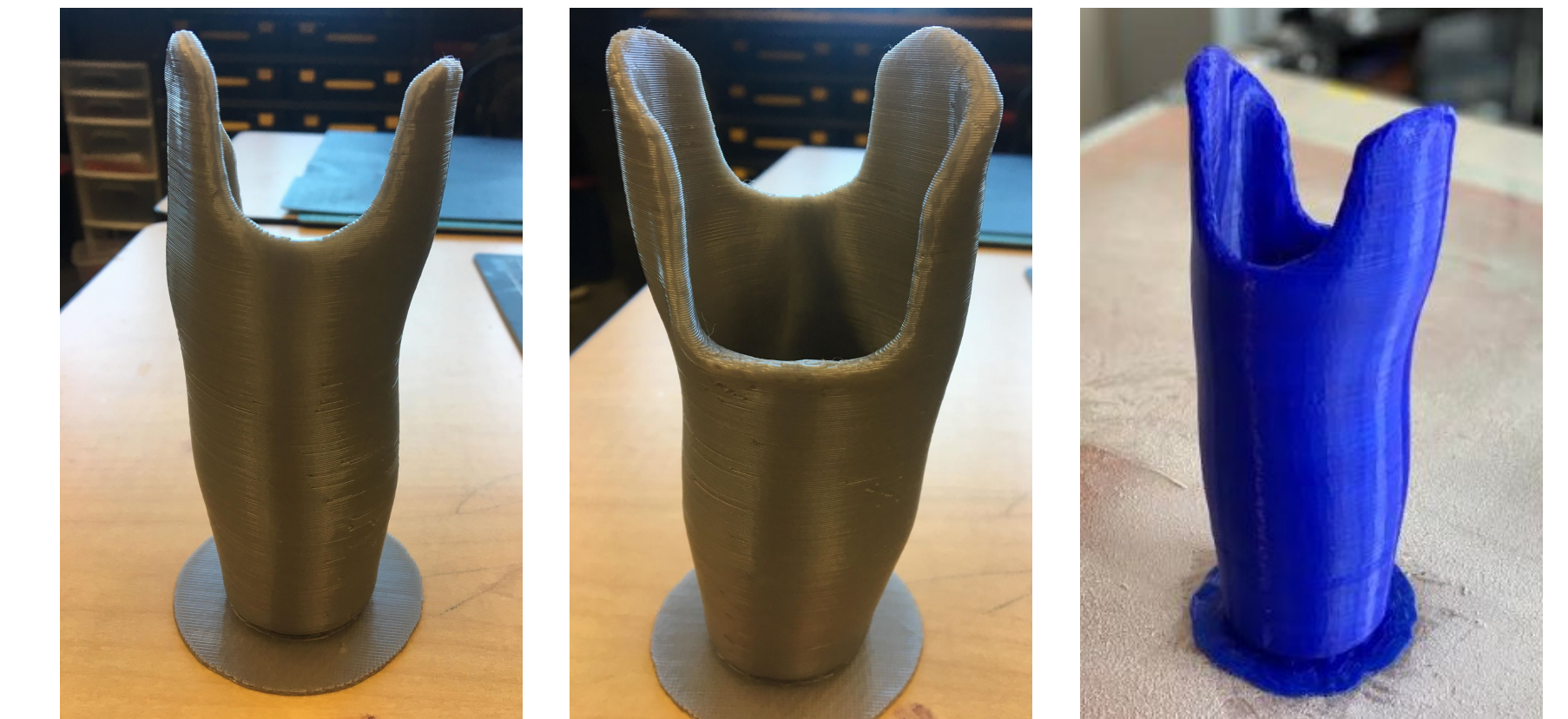


Figure 10: Half scale (grey) and Full scale (blue) 3D Printed Sockets.

- ❖ Used polylactide (PLA) to 3D print
- ❖ Half-scale model took 5 hours (grey)
- ❖ Full-scale model took 60 hours (blue)
- ❖ Scaling was slightly small
- ❖ Extended sides could be more even

### Cloudcompare

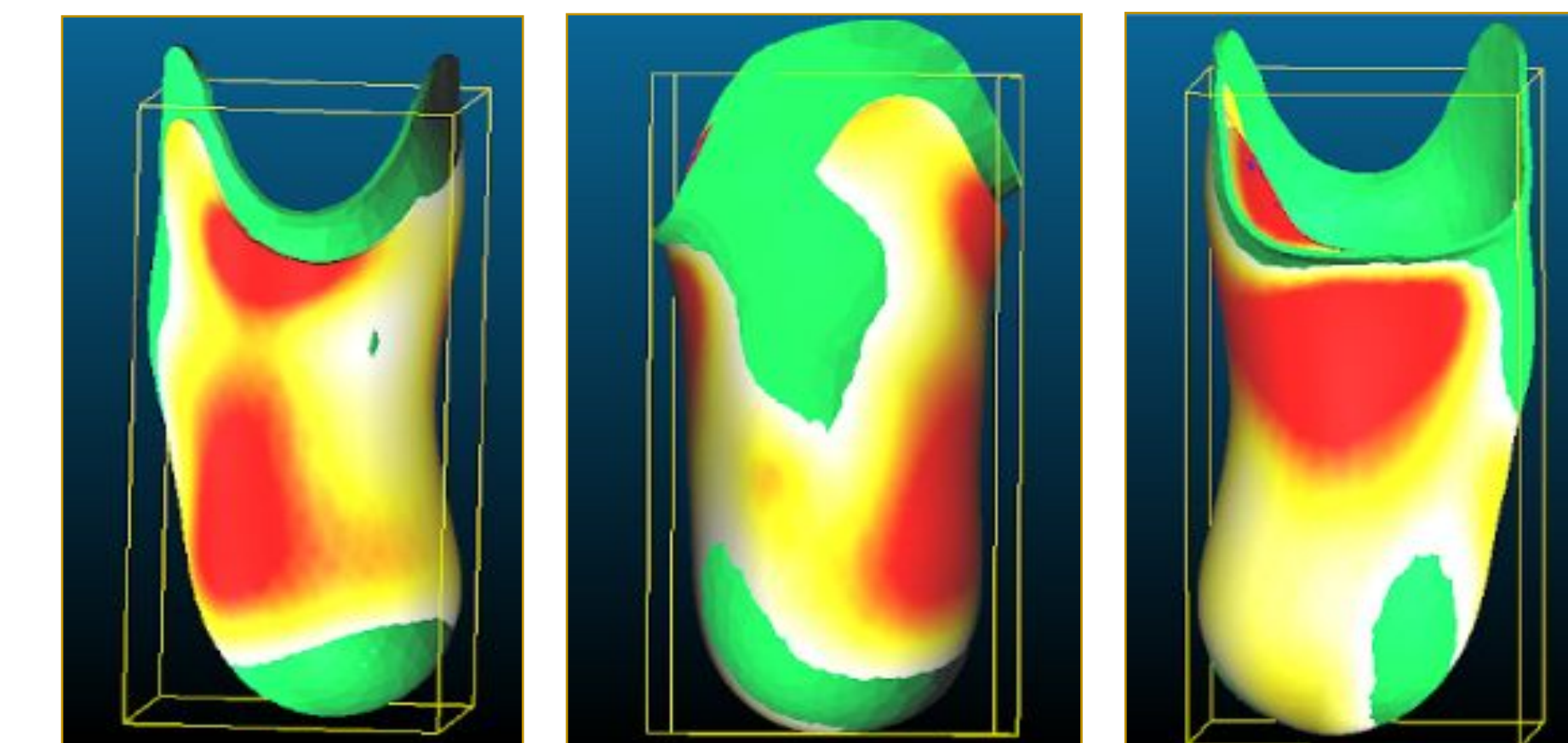


Figure 11: Comparison of Our Socket vs. Prosthetist's Socket.

- ❖ Compared prosthetist's socket to our own
- ❖ Interior mostly within 5mm
- ❖ Our socket was slightly smaller

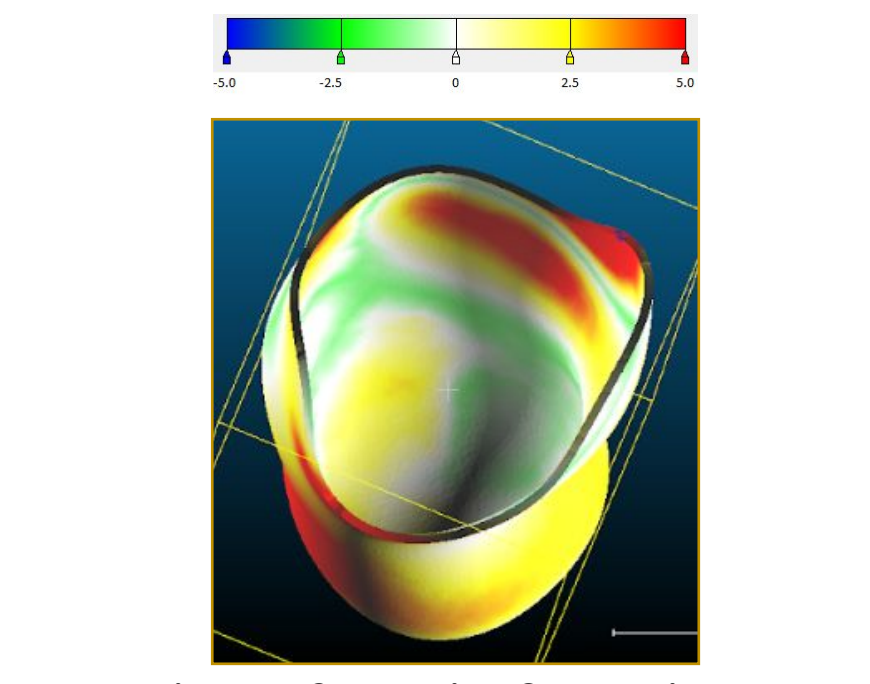


Figure 12: Interior Comparison.

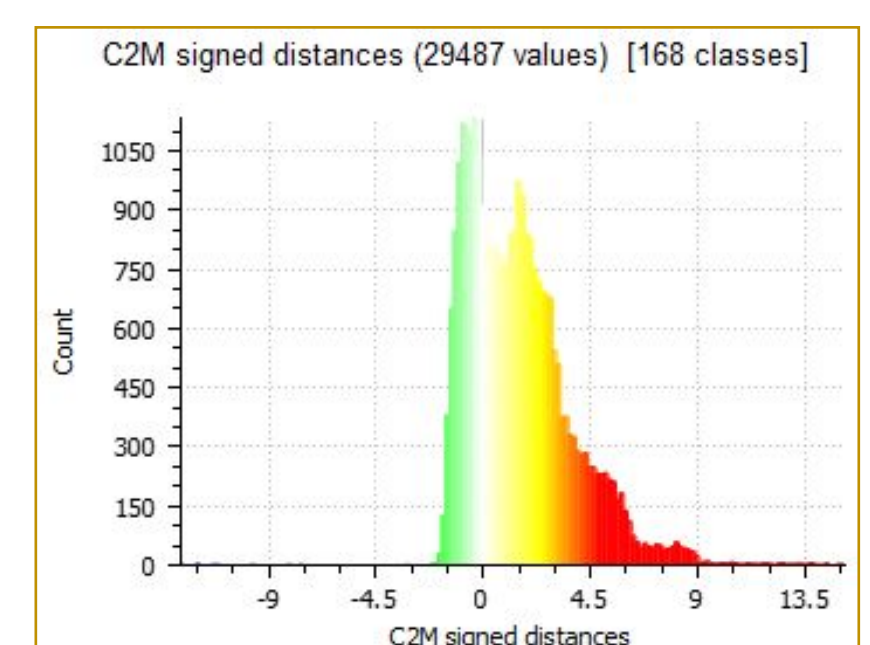


Figure 13: Histogram of Comparison.

## Conclusions & Future Work

- ❖ Socket design printed well with minimal support material
- ❖ The size of our socket model matched close to the professional socket
- ❖ In the future, we want to
  - Integrate a suspension system to keep the socket on the limb
  - Test fit and comfort of the socket on the user

## References

- (1) Marino, M., Pattni, S., Greenberg, M., Miller, A., Hocker, E., Ritter, S., & Mehta, K. (2015). Access to prosthetic devices in developing countries: Pathways and challenges. In *Proceedings of the 5th IEEE Global Humanitarian Technology Conference, GHTC 2015* (pp. 45–51). Institute of Electrical and Electronics Engineers Inc. <https://doi.org/10.1109/GHTC.2015.7343953>
- (2) Dou, Jia, Suo, Wang, Zhang, et. al. (2006). Pressure distribution at the stump/socket interface in transtibial amputees during walking on stairs, slope and non-flat road. *Clinical Biomechanics*, 21, 1067-1073.
- (3) "Prosthetics Get an Upgrade with 3D Printing." *The Garage*, HP, 21 Mar. 2019, <http://garage.ext.hp.com/us/en/innovation/hp-3d-printing-prosthetics.html>.
- (4) "Transtibial Sockets." Australian Physiotherapists in Amputee Rehabilitation, Sept. 2010, [http://www.austpar.com/portals/prosthetics/transtibial\\_sockets.php](http://www.austpar.com/portals/prosthetics/transtibial_sockets.php)
- (5) "Symphonie Aqua System - The most advanced socket casting system in the world." *The London Prosthetic Centre*, 03 Mar. 2016, [http://thelondonprosthetics.com/news/symphonie\\_aqua\\_system\\_the\\_most\\_advanced\\_socket\\_casting\\_system\\_in\\_the\\_world/](http://thelondonprosthetics.com/news/symphonie_aqua_system_the_most_advanced_socket_casting_system_in_the_world/)